

THE IMPACT OF PARAMETER VARIATION, EXPERIMENTAL DATA AND UNCERTAINTY QUANTIFICATION FOR COMPLEX BIOMECHANICAL PROBLEMS EXAMPLIFIED FOR AAA



Jonas Biehler[†], Michael W. Gee[‡], Wolfgang A. Wall[†]

[†]Institute for Computational Mechanics,
[‡]Mechanics & High-Performance Computing Group,
 Technische Universität München



Introduction

AAA rupture risk prediction using FEM

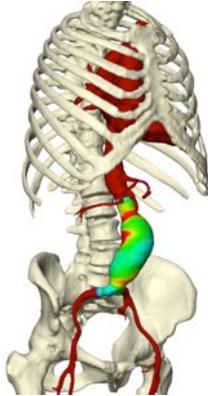
- Computational rupture risk indicators, e.g., peak wall stress are superior to the diameter criterion [1].
- Most "patient-specific" models are based on population averaged model parameters.

Existing uncertainties

- Computational geometries, e.g., wall thickness
- Boundary conditions, e.g., intra luminal pressure
- Physical parameters, e.g., constitutive parameters

Towards more reliable rupture risk prediction

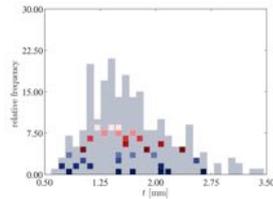
- In absence of truly patient-specific parameters: include uncertainties in the FEM analysis
- Here uncertain wall thickness is considered and its impact on peak wall stress is studied. For uncertain constitutive parameters, see [2].



Probabilistic models of AAA wall

Experimental research

- Experimental measurements reveal significant inter- and intra-patient variations for wall thickness
- Probability distribution for thickness t can be estimated from histogram
- 29 supplementary patient- and specimen-specific parameters v were gathered in addition to thickness measurements and tensile test data.



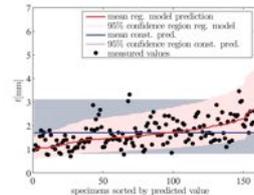
Histogram of measured thickness values. Squares of same color indicate measurements from same patient

Harnessing non-invasive information

- The supplementary data can be harnessed by Bayesian regression models to obtain non-invasive predictions of patient-specific wall thickness and other quantities [3].
- Using Gaussian process (GP) regression GP prior:

$$\log t(\mathbf{v})|\theta_m, \theta_k \sim \mathcal{GP}(m_t(\mathbf{v}; \theta_m), k_t(\mathbf{v}, \mathbf{v}'; \theta_k))$$
- GP is conditioned on available data D .
- The hyper-parameters θ_m, θ_k are obtained by maximization of the marginal likelihood [5].
- Gaussian predictive distribution for $\log t$ depends on non-invasively accessible parameters v^* of particular patient:

$$p(\log t^* | v^*, D) = \mathcal{N}(m_t^*, \sigma_t^{*2})$$
- Regression model allows more accurate prediction of wall thickness with reduced variance, i.e., uncertainty about t than direct estimation.



Regression model predictions and measured values for wall thickness of excised specimens. Explanatory variables used in regression model: sex, age, ruptured, subrenal diameter, CKD, DM, creatinin, erythrocytes, thrombocytes, sodium, urea, MCH, MCHC, distance to bifurcation, thrombus thickness, and NORD.

Considered probabilistic wall thickness models

- Spatial, intra-patient variations can only be captured with random field model.
- Positivity constraint: (marginal) Gaussian distribution for $\log t$
- Three different probabilistic wall models are considered:
 - Model A: Random field model, parameters estimated from available thickness measurements
 - Model B: Random field model, parameters obtained from GP regression model which predicts wall thickness distribution
 - Model C: Random variable model, distribution parameters estimated from available thickness measurements

Propagation of uncertainties

Bayesian multi-fidelity Monte Carlo

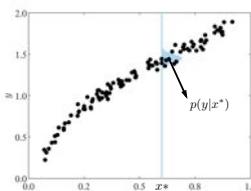
- Incorporation of low-fidelity models [2][4]
- Probabilistic link between low-fidelity model x and high-fidelity y model obtained with Bayesian regression.

$$\pi_y(y) = \int p(y|x)\pi_x(x)dx$$

- Accurate and efficient for problems with high stochastic dimension
- Here: low-fidelity model simply assumes a linear relationship between local wall stress and local wall thickness.

Gaussian process Bayesian surrogate model

- If wall thickness is modeled as random variable, Bayesian surrogate models are more suitable.



Schematic representation of correlation between low-fidelity and high-fidelity model output.

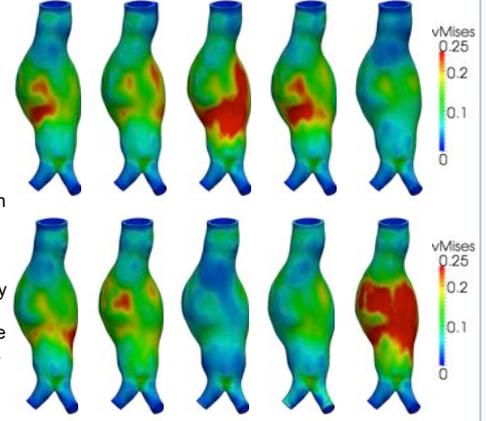
Results for exemplary AAA geometry

Patient-specific AAA model

- Full nonlinear patient-specific model with ca. 380.000 degrees of freedom
- Nonlinear constitutive models of AAA wall and ILT based on [6] and [7]
- Realizations of random wall thickness are created at runtime using pseudo-structure approach.
- Quantity of interest: von Mises peak wall stress

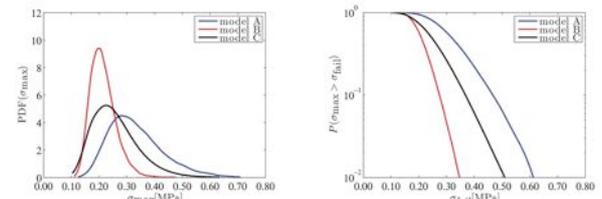
Impact on wall stress

- High variability for wall stress and peak wall stress
- Large variability in thickness can result in drastically different stress patterns for both of the random field models A and B.
- If model C is used, stress pattern is largely determined by geometric features and the location of peak stress stays the same.



Resulting von Mises stress σ_{vM} [MPa] for 10 realizations of model A

Probability distribution of peak wall stress



Probability distribution for peak wall stress. Left: PDF. Right: failure probability for threshold σ_{fail}

	$E[\sigma_{max}]$ [MPa]	$var[\sigma_{max}]$	95% q. of σ_{max} [MPa]
model A	0.333	0.0094	0.516
model B	0.215	0.0021	0.298
model C	0.259	0.0069	0.412

- Model A exhibits significantly larger variance than model B.
- Uncertainty about peak wall stress can be reduced by using regression models to predict the wall thickness distribution.
- Distributions for model A and model C are different, i.e., the choice of probabilistic wall model affects probability distribution of peak wall stress.
- Efficient solution of UQ problem through Bayesian multi-fidelity Monte Carlo or Gaussian process surrogate models reduces costs to acceptable level.

Conclusion and outlook

- We quantified uncertainty about peak wall stress in AAA due to uncertain wall thickness, inclusion of additional uncertain parameters is possible.
- Random variable models for the thickness can be overly simplistic
- Regional spatial variations in wall thickness are important and should not be neglected
- Study with larger patient cohort is needed to confirm preliminary results.
- 95% quantile could serve as worst case estimate for peak stress, however, definition of a probabilistic failure measure is necessary.

References:

- [1] Maier A., Gee M.W., Reeps C., Pongratz J., Eckstein H.H., Wall W.A., A comparison of diameter, wall stress, and rupture potential index for abdominal aortic aneurysm rupture risk prediction. *Annals of Biomedical Engineering* 2010; 38(10):3124–3134.
- [2] Biehler J., Gee M.W., Wall W.A. (2014). Towards efficient uncertainty quantification in complex and large-scale biomechanical problems based on a Bayesian multi-fidelity scheme. *Biomechanics and Modeling in Mechanobiology*, 2015, 14(3):489–513.
- [3] Biehler J., Kehl, S., Gee, M.W., Tanios, F., Pelisek, J., Maier, A., Reeps, C., Eckstein, H.H., Wall, W.A., Non-invasive prediction of wall properties of abdominal aortic aneurysms using Bayesian regression, 2015, in preparation.
- [4] Koutsourelakis P., Accurate uncertainty quantification using inaccurate models. *SIAM Journal of Scientific Computing* 2009, 31(5): 3274–3300.
- [5] Williams, C. K., Rasmussen, C. E., *Gaussian processes for machine learning*, 2006, MIT Press.
- [6] Raghavan, M. L., Vorp, D. A., Toward a biomechanical tool to evaluate rupture potential of abdominal aortic aneurysm: identification of a finite strain constitutive model and evaluation of its applicability. *Journal of Biomechanics*, 2000, 33(4), 475–482.
- [7] Gasser, T. C., Gorgülü, G., Folkesson, M., Swedenborg, J., Failure properties of intraluminal thrombus in abdominal aortic aneurysm under static and pulsating mechanical loads. *Journal of Vascular Surgery*, 2008, 48(1), 179–188.